

Oral Controlled Release Formulations

Sheri Shamblin



We provide premium technical consulting services for the design and development of immediate-release and controlled release medicines. Our primary focus is on small molecule oral drug products.

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Sheri L. Shamblin, PhD

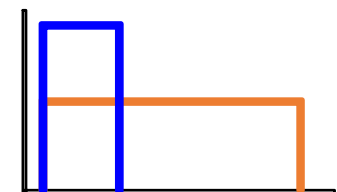
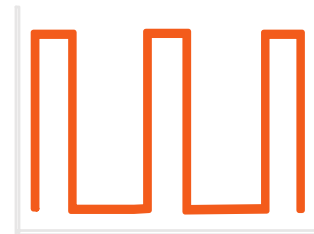
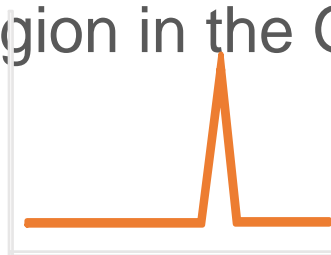
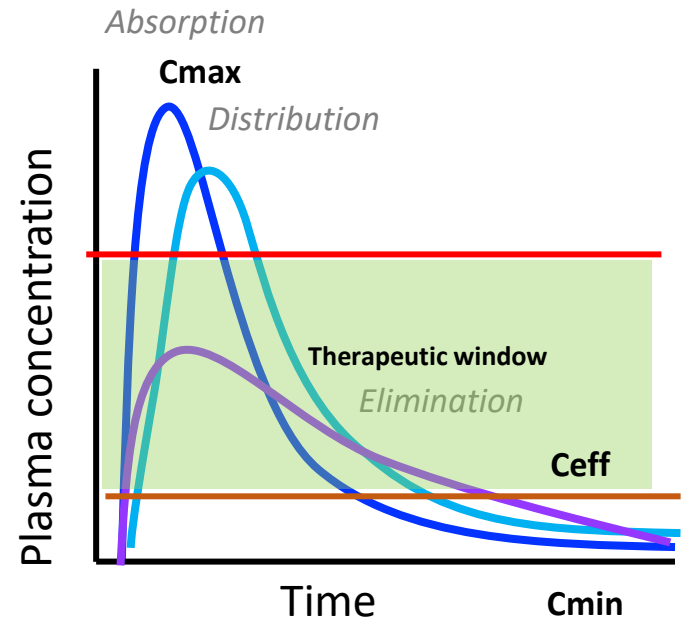
- Principal consultant for Aleurites.
- Over 28 years working in drug development at Pfizer Inc.
- Expertise in the design and development of oral controlled release formulations and formulations to increase solubility and bioavailability.

What you will learn

- Typical drivers for use of oral controlled release (CR) formulations.
- An overview of standard oral CR technologies.
- What CR technology is appropriate for your drug.
- Tips and tools for formulation development and clinical evaluation.

Drivers for Controlled Release

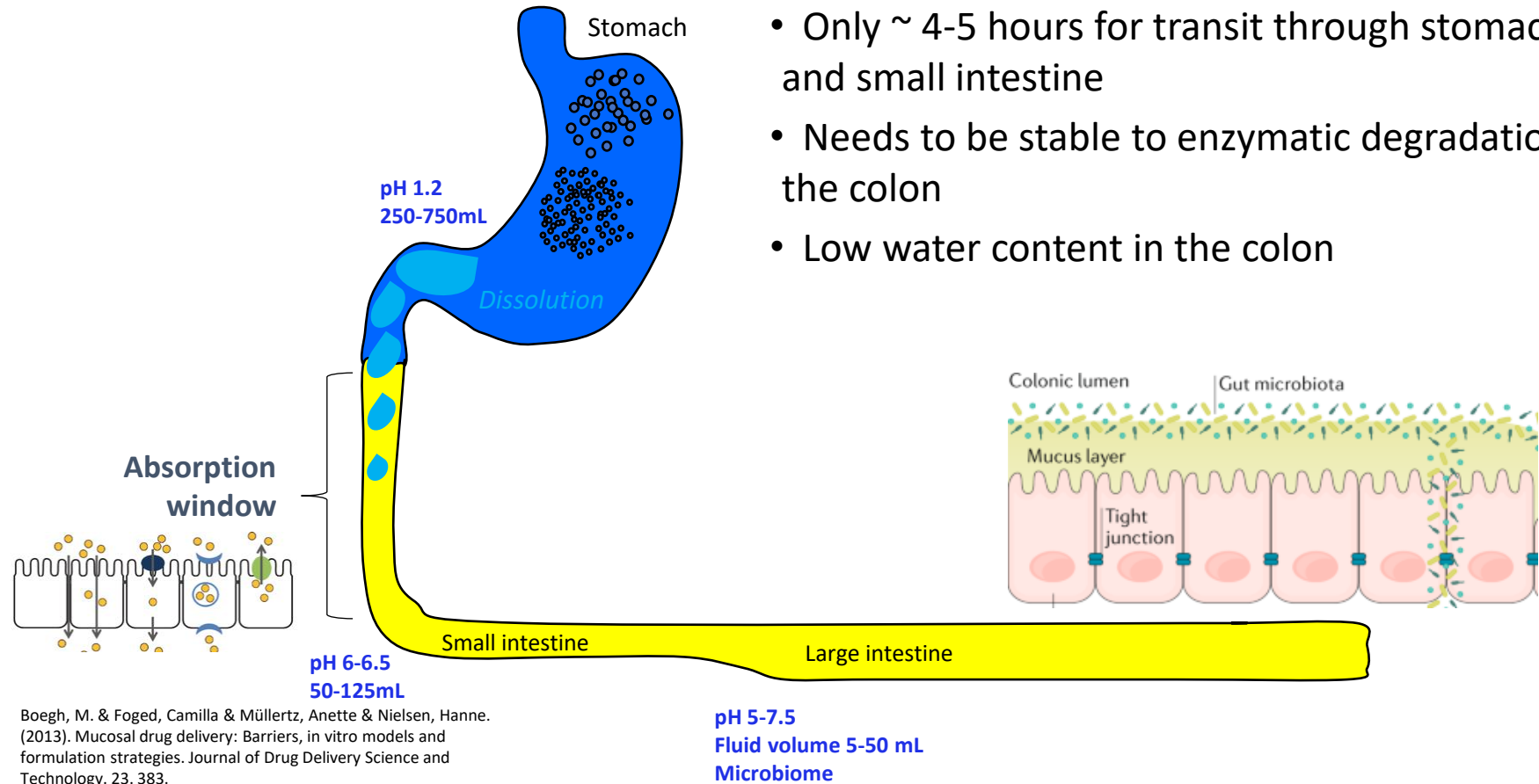
- Reduce the frequency of dosing
 - TID (3 times a day) to BID (2 times a day) or QD (once a day)
- Reduce side-effects
 - Local, e.g., irritation in GI
 - Systemic
 - reduce “rate of rise” of plasma levels
 - reduce C_{max}/C_{min}
- Increase efficacy
- Decrease drug degradation in stomach
- Delivery to OR around a specific region in the GI tract



Oral CR Delivery and GI Physiology

$$\text{Dose Volume (mL)} = \frac{\text{Dose (mg)}}{\text{Solubility} \left(\frac{\text{mg}}{\text{mL}} \right)}$$

- Colonic absorption is **LIKELY** needed for most CR dosage forms
- Only ~ 4-5 hours for transit through stomach and small intestine
- Needs to be stable to enzymatic degradation in the colon
- Low water content in the colon



Boegh, M. & Foged, Camilla & Müllertz, Anette & Nielsen, Hanne. (2013). Mucosal drug delivery: Barriers, in vitro models and formulation strategies. Journal of Drug Delivery Science and Technology. 23. 383.

Long duration = more challenging

Before you begin formulating: Controlled Release Feasibility

Solubility

- Dose, solubility and duration
- Role of pKa and pH for ionizable drugs

Permeability

- Differences in regional absorption along the GI tract
- Efflux mechanisms, PGP

Stability

- Chemical stability (polymers for matrix and functional coatings)
- Enzymatic stability (in vivo)

Metabolism

- Rate of elimination ($t_{1/2}$)
- Mechanism of elimination and extent of first-pass

Thombre, A. G. (2005). Assessment of the feasibility of oral controlled release in an exploratory development setting. *Drug Delivery Today*, 10(17), 1159–1166.

Assessment of Clinical Success with CR

Factor	
Dose	<1mg
	10-250mg
	>>250-300mg
Dose:Solubility (Dose volume)	<1mL
	100-1000 mL
	>1000 mL
	>10,000 mL
Regional Permeability	Good- $P_{app} > 10^{-5}$ cm/s
	Moderate $P_{app} 10^{-5} - 10^{-6}$ cm/s
	Poor $P_{app} < 10^{-6}$ cm/s
PK or PD half-life	>>10h
	2-10 h
	<1-2

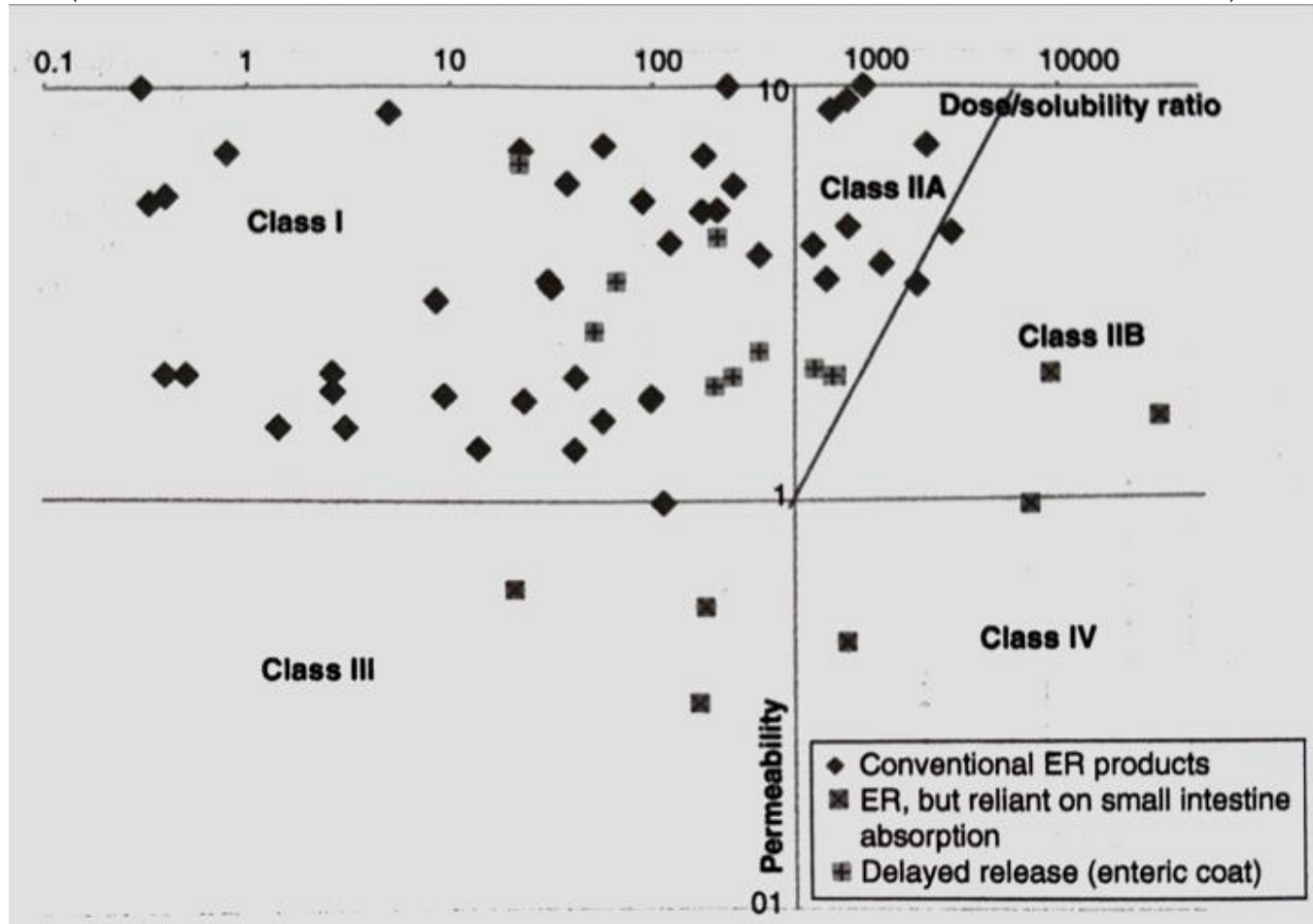
Stability, absorption pathways, role of efflux and metabolic pathways are also critical

Thombre, A. G. (2005). Assessment of the feasibility of oral controlled release in an exploratory development setting. *Drug Delivery Today*, 10(17), 1159–1166.

Developability Classification System and Commercial MR Products



Feasibility based on Thombre, 2005.



Butler, J.M., "The Application of Biopharmaceutics Classification Systems to Modified-Release Formulations", in *Oral Drug Delivery for Modified Release Formulations, First Edition, 2022, Wiley & Sons.*

Oral Controlled Release Technologies

Increasing complexity

- Matrix Tablet

- Polymer matrix controls drug release
- Most common oral CR technology used for marketed drugs

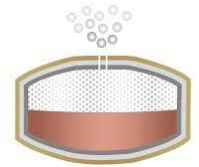
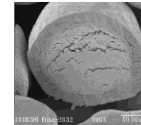
- Multiparticulates

- Particulates ranging from 0.2 – 3.0mm
- Includes beads, granules, minitables microspheres
- Control through multiparticulate and/or functional coating



- Delayed Release (enteric coated)

- Tablets (IR or CR)
- Multiparticulates (bead or minitables)



- Osmotic Pump

- Constant rate of delivery driven by flux of water across a semi-permeable membrane

- Gastric Retentive

- Polymers that expand or swell
- Large size prevents passage through pylorus



Controlling release by controlling diffusion

Fick's First Law

$$\frac{dQ}{dt} = \frac{DAk}{h} (C_x - C_o)$$

D = diffusion coefficient (depends on viscosity, size of diffusing species)

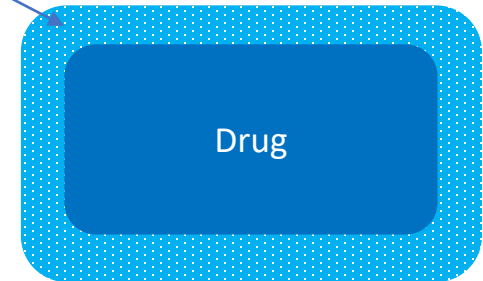
A = surface area of membrane

k = partition/permeability coefficient

h = membrane thickness

C_x-C_o = concentration difference

Barrier to diffusion created by gel, coating, porous membrane



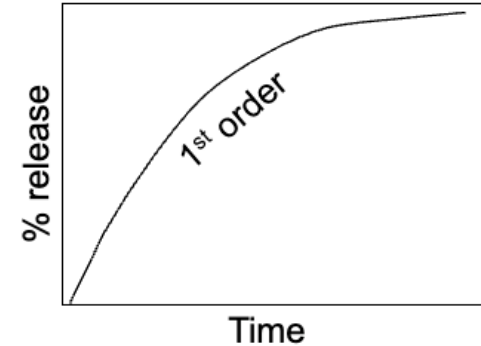
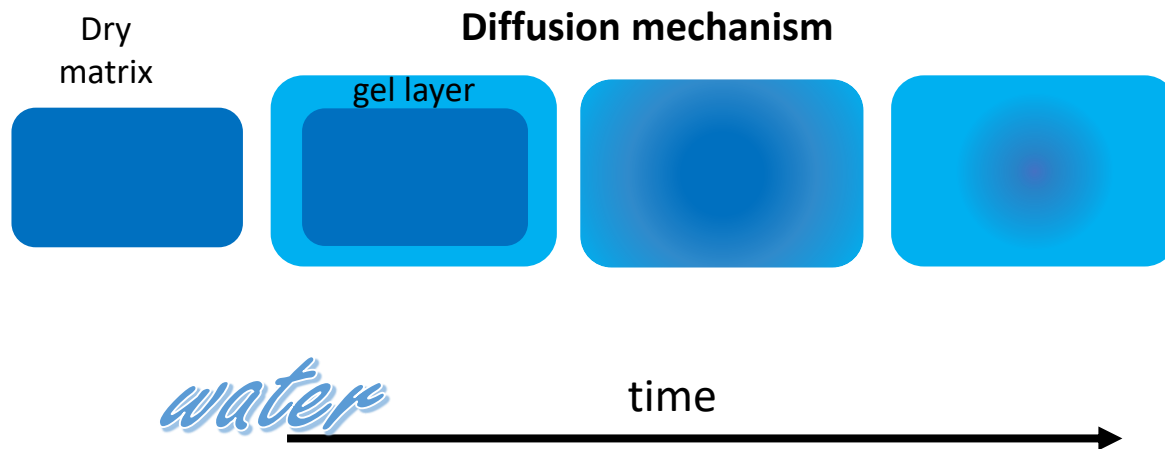
Controlling drug diffusion

- Diffusion of drug across a membrane
- Diffusion of drug through a viscous matrix or gel
- Porous diffusion through a hydrophobic matrix (multiparticulate bead, granules)
- Controlled diffusion of water into a tablet through a semi-permeable membrane to create an osmotic pump that delivers drug

Matrix Tablets

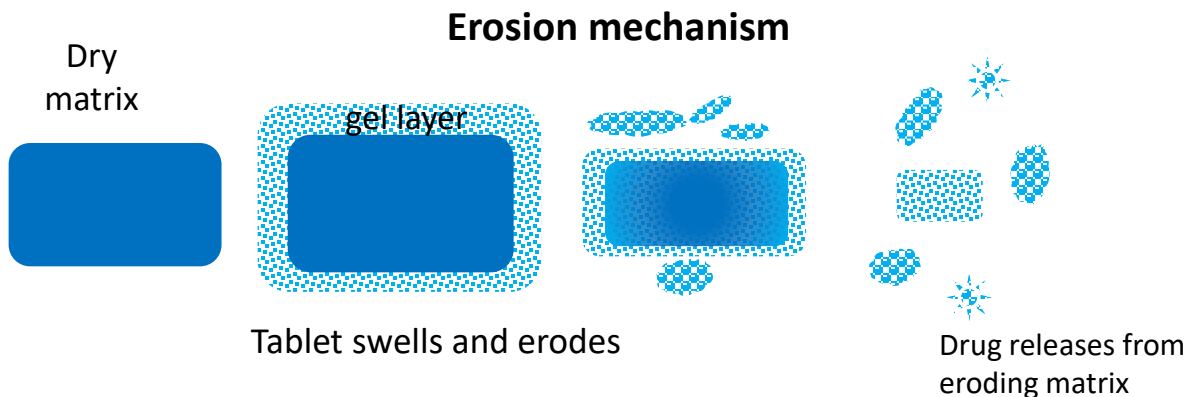
Matrix Tablets: Mechanism of Control

Homogeneous blend of drug, hydrophilic or hydrophobic polymers, soluble and insoluble excipients



$$\frac{dM}{dt} \approx C_d A l D_{eff}$$

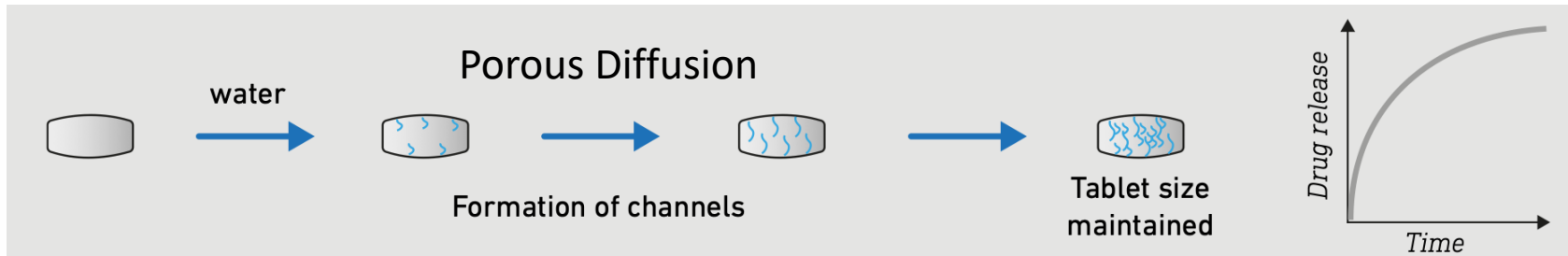
Drug dissolves and diffuses through viscous gel created by polymer matrix



$$\frac{dM}{dt} \approx kA$$

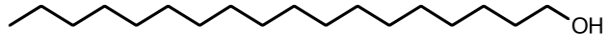
Undissolved drug weakens polymer gel resulting in erosion of the hydrate matrix

Wax Matrix: Mechanism of Release



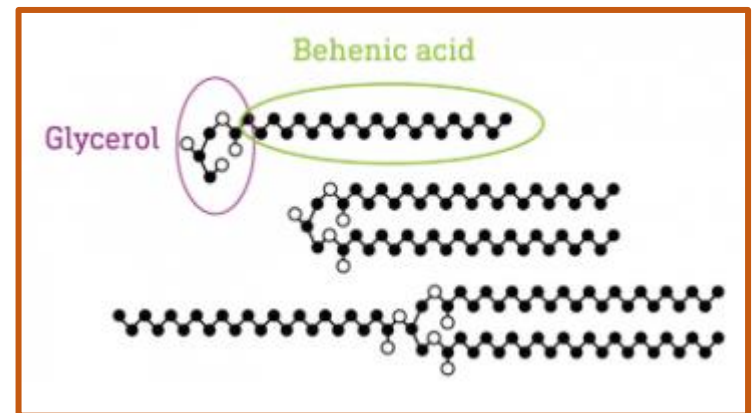
Fast release

Stearyl alcohol



Slow release

Glyceryl behenate



Matrix Tablets

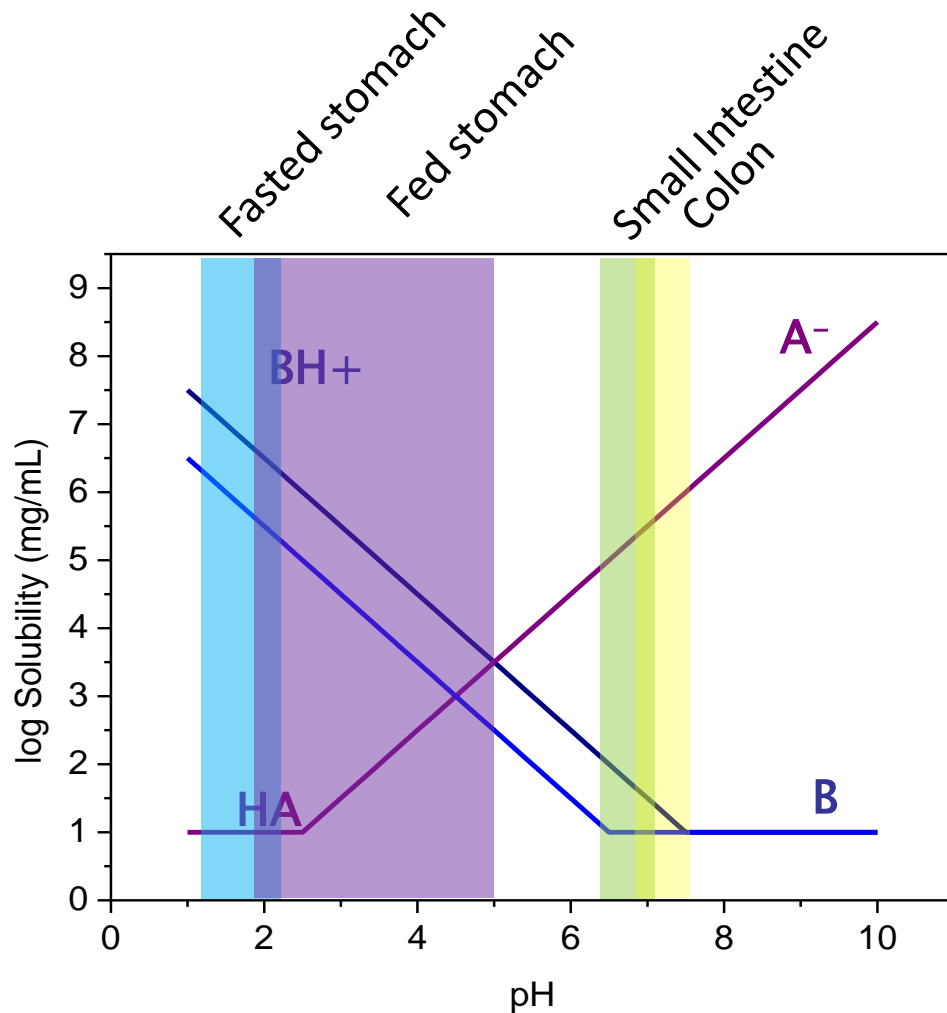
Attributes

- Simple to manufacture
- Wide-selection of polymers and waxes available
- No functional coatings required
- Can be coated to provide a delayed CR profile.

Challenges

- Release rate depends on drug solubility in aqueous environment
- Variable release for ionizable drugs
- Eroding matrix tablets are sensitive to food/digestion and can have a food effect
- In vitro release rate may not be predicted of in vivo release and performance

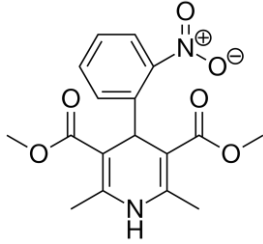
Ionizable Drugs and Solubility



- Ionizable drugs have pKa's from 3-7, drug solubility will change as the drug/dosage form move through the GI tract.
- For matrix tablets, the change in drug solubility will cause a change in release rate, and even mechanism.

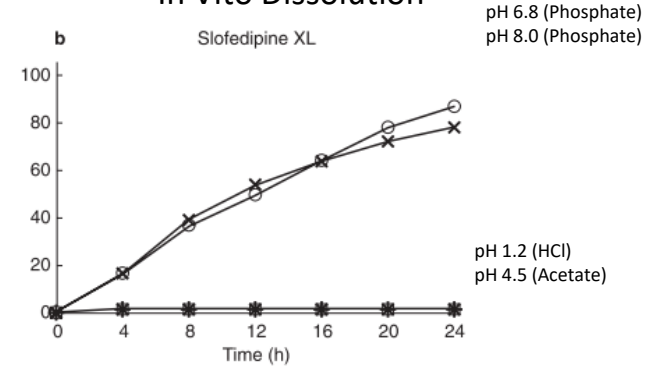
Li, X., Jasti, B. "Design of Controlled Release Drug Delivery Systems", McGraw-Hill, 2006

Controlled Release of Nifedipine

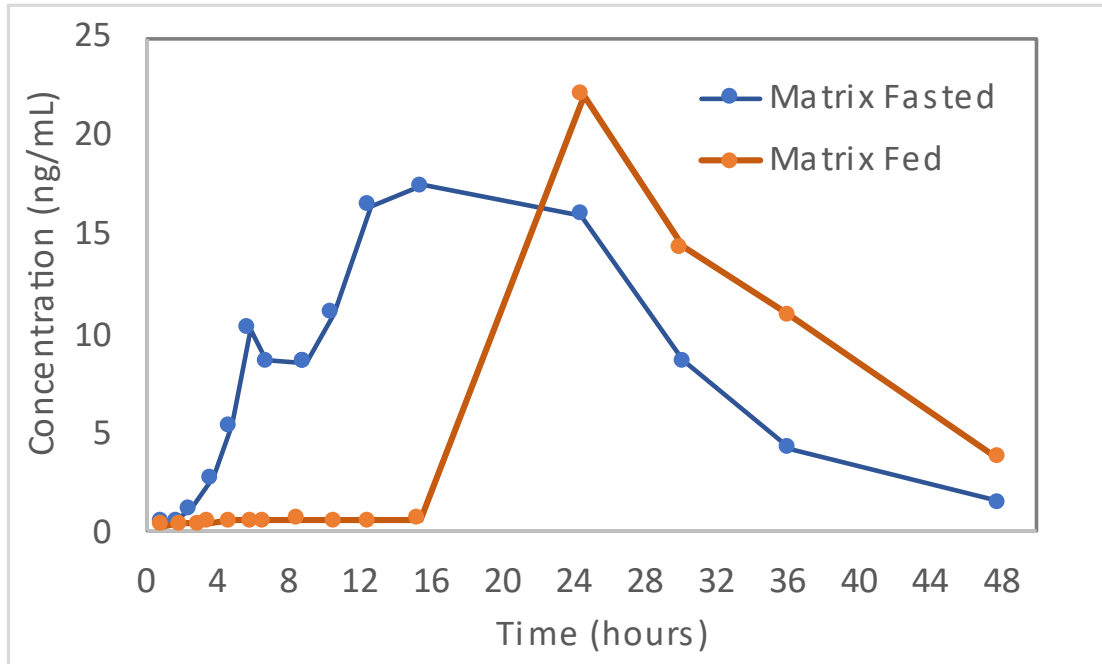


$pK_a = 3.93$ (weak acid)
10ug/mL (water)

In Vito Dissolution



PK Profile of Nifedipine in Humans (n=24)



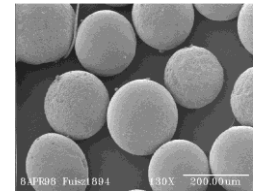
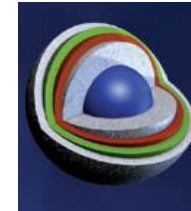
Friedrich, H. (2004). Improvement of solubility and stability of poorly soluble drugs. In: Ph.D. Dissertation. Berlin, Germany: Freie Universität Berlin.
Freidrich et al (2005). *Drug Dev and Ind. Pharmacy*, v31, 8, p 718-728

Multiparticulates

Multiparticulates: Flexibility and versatility

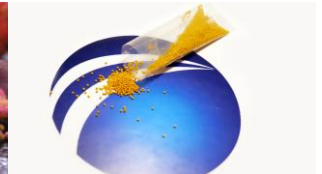
Types of multiparticulates:

- Wax/polymer matrix beads
- Drug layered bead
- Granules
- Minitablets
- Coated or uncoated



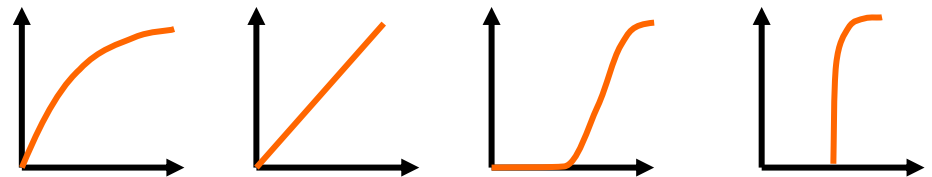
Presentations to the Patient

- Capsule
- Sachet
- Stick pack



Coatings:

- Enteric (pH release)
- Time release
- Semipermeable (osmotic)



Multiparticulates

Attributes

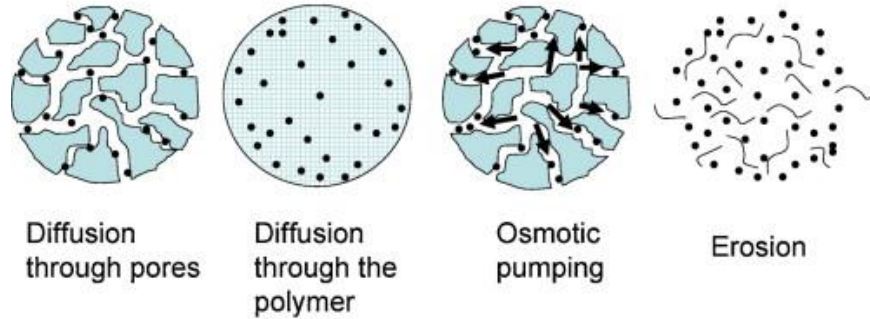
- Broad category that includes many types of particulates (0.2mm – 3.0mm)
- Reproducible GI transit (more consistent with or without food)
- Wide range of release profiles possible: Delayed (enteric), Sustained, Pulsed, or IR+CR
- Well-suited for combination drugs
- Pediatric/geriatric dosage form
- Offers versatility in release profile
- Flexibility in dose and presentation

Challenges

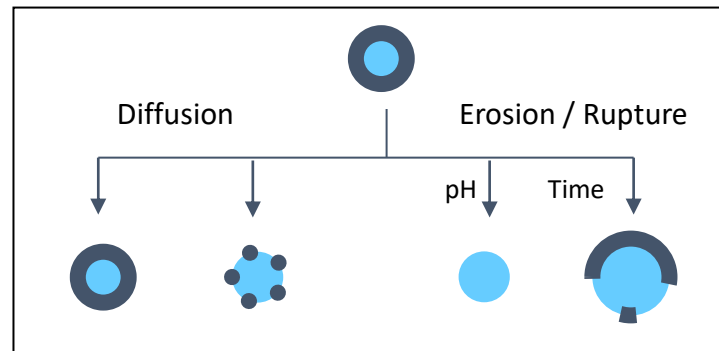
- Complex manufacturing compared to monolithic matrix tablets
- Drug loadings are on the low side, typically <30%

Multiparticulates: Mechanisms of drug release

CR Multiparticulates

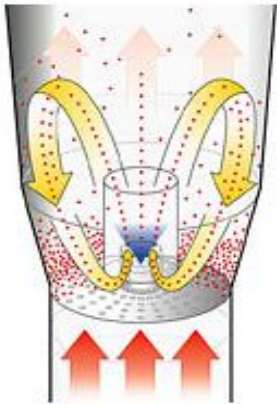


Film coated beads



Manufacturing Multiparticulates

Fluid Bed



Cellets
(microcrystalline cellulose beads)

Photo: Cellet.com

- CR granules
- Drug layering on inert beads
- Functional coating of beads, granules, minitables

Extrusion

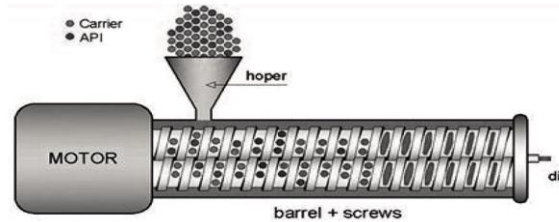


Image: Aleksovski et al, 2016,
Macedonian pharmaceutical bulletin

- CR granules or pellets
- Feed for congealing

Compression of Minitablets



Photo: Tabletsandcapsules.com

- CR granules or pellets
- Feed for congealing

Congeval Spin or Spray

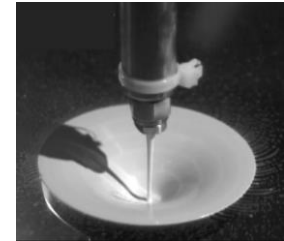


Photo: SWRI

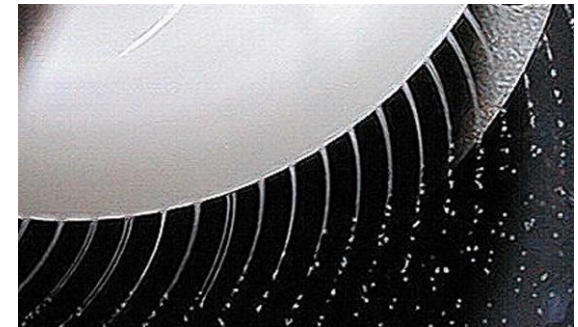


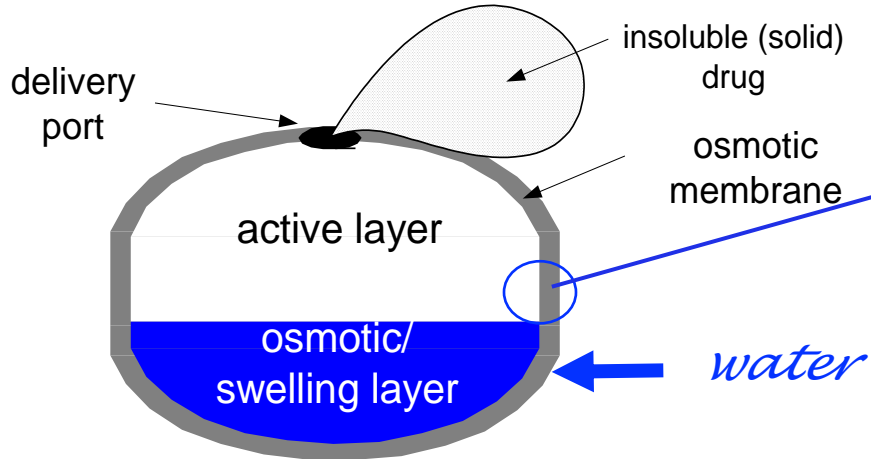
Photo: SWRI

- Microspheres – 200-500 um (spinning disk)
- Microspheres – 500-1000 um (spray-congeal)

Osmotic Tablets

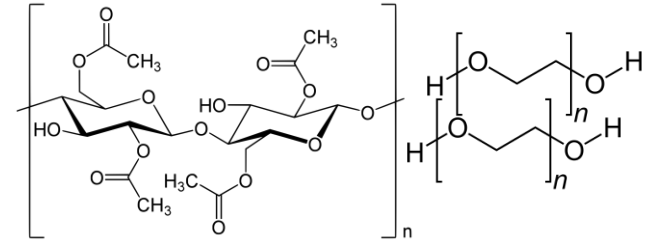
Osmotic Tablet Technology

Bilayer Osmotic Tablet



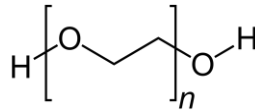
Drug release is controlled by the semi-permeable osmotic membrane and an osmogen (NaCl)

Cellulose acetate and polyethylene glycol



Active layer:

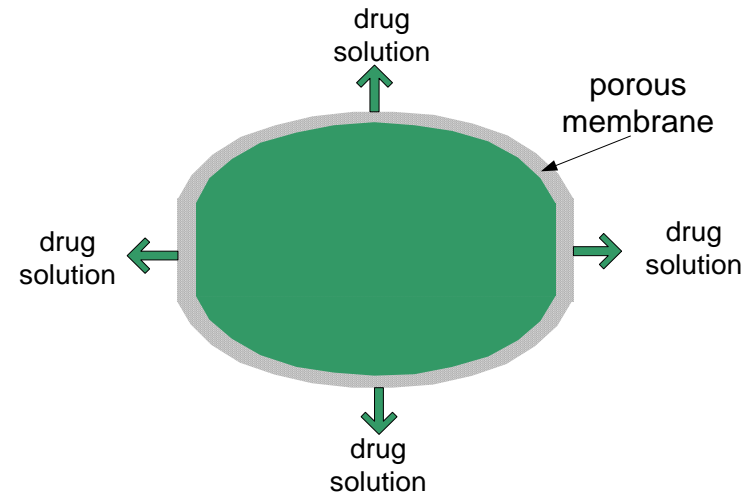
- Drug
- Polyethylene oxide (2M)



Swelling layer:

- NaCl
- Polyethylene oxide (5M)
- Blue Lake #2

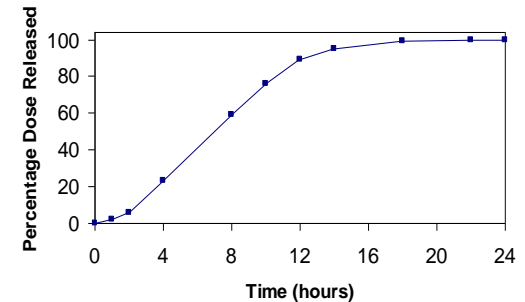
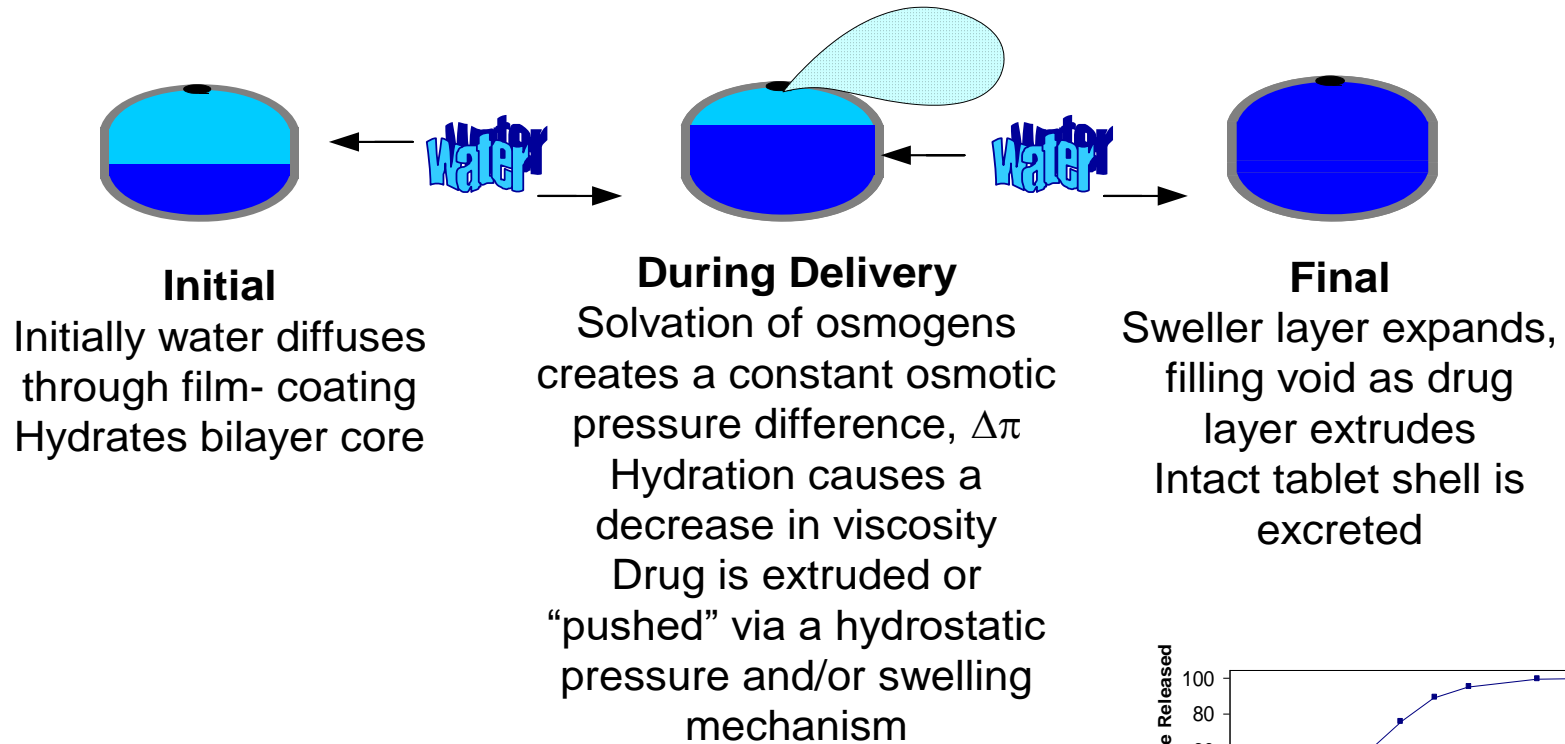
Monolithic Osmotic Tablet



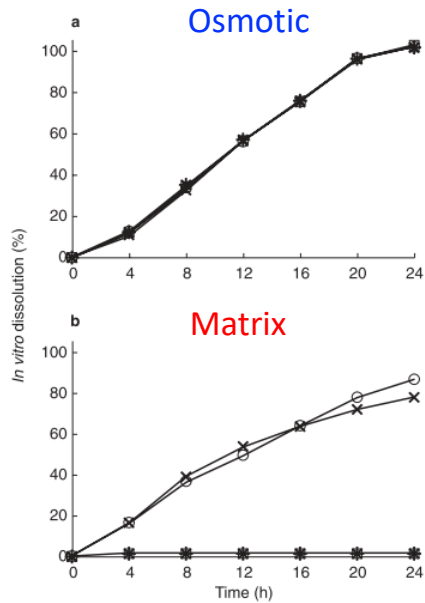
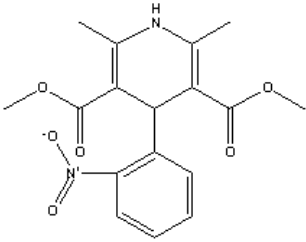
Shamblin, S. L. (2010). Controlled release using bilayer osmotic tablet technology: reducing theory to practice. Oral Controlled Release Formulation Design and Drug Delivery: Theory to Practice, 129–153.



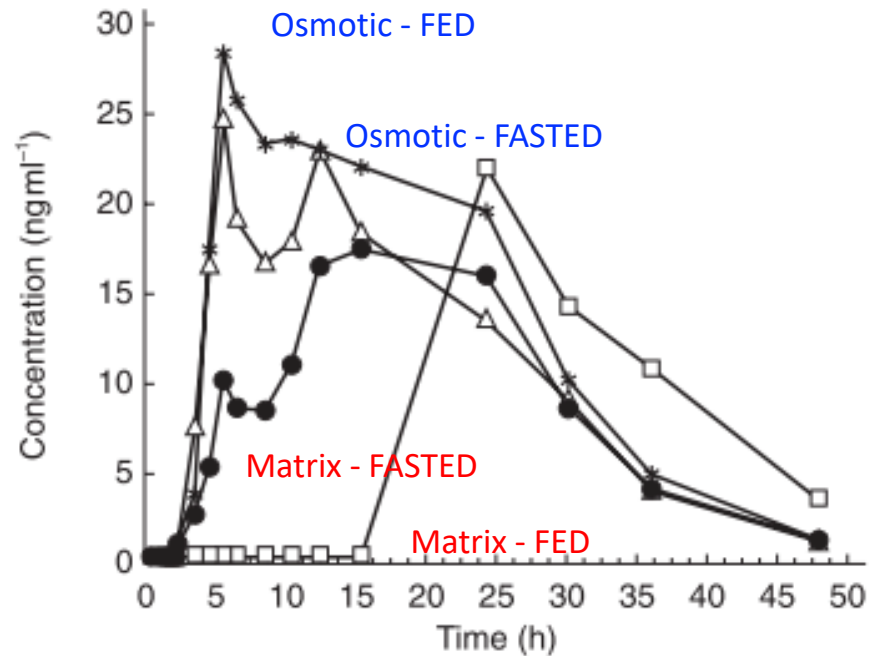
Generic Mechanism of Delivery For Osmotic Drug Delivery Systems



Nifedipine: Osmotic vs Matrix Tablet



PK Profile of Nifedipine in Humans (n=24)



Osmotic Tablets

Attributes

- Delivers drug via osmotic potential typically in a zero-order fashion
- Drug release independent of pH/ stirring even for low solubility and ionizable drugs
- Applicable to drugs independent of their solubility
- Good in-vitro/in-vivo predictive tests – speed development and minimize iterations

Challenges

- Complex manufacturing Solvent coatings
- May require laser-drilling and requires solvent coating capability
- May require layered tablet cores and hole(s) in coating.
- Drug loadings are on the low side, typically <30%
- Can have a lag time to initial drug delivery
- Not well suited to multiple profiles or combination therapies.

Additional ways to control drug release

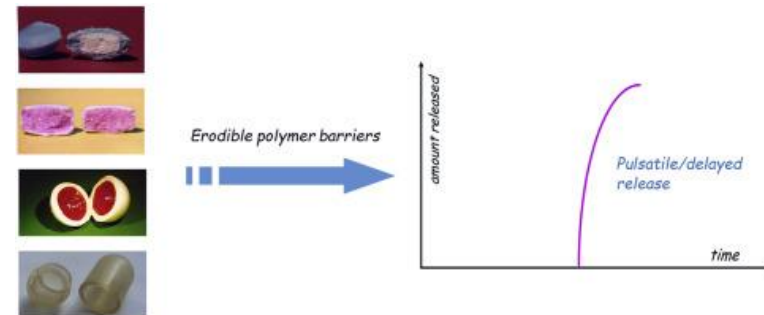
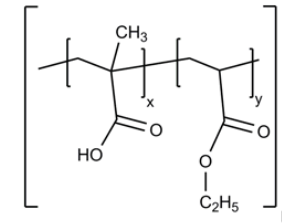
- Delayed drug release (pH, time)

- Enteric polymer coatings prevent drug release in the stomach
- Reverse enteric polymer coatings that prevent drug release in neutral environment in the mouth.
- Use of erodible polymer coatings/barriers to slow or delay release
- Control obtained using coating type and thickness

- Gastric-retentive

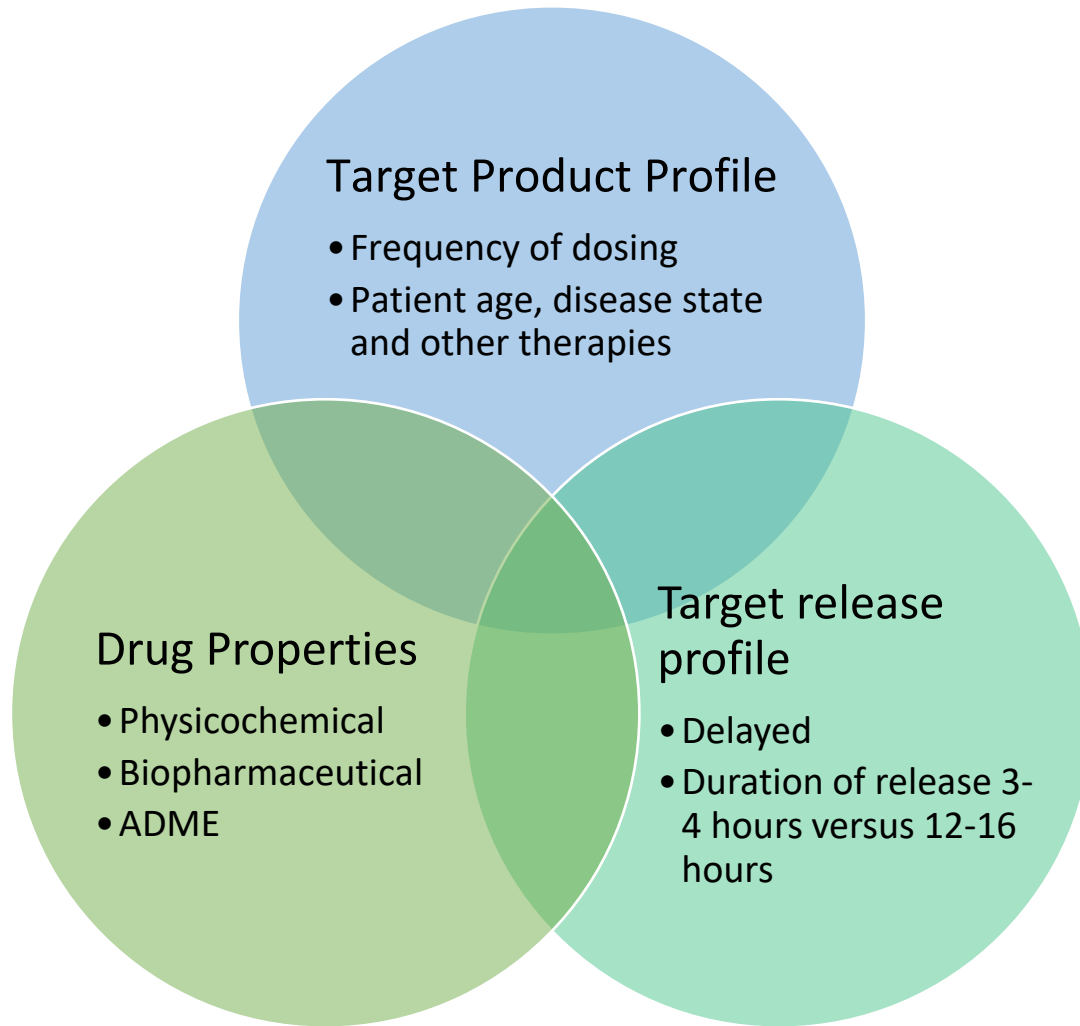
- Designed to remain in stomach using swelling, density or muco-adhesion
- Control of drug release using polymers, hydrogels to slow drug release
- Limits drug absorption to the duodenum

EUDRAGIT® L 30 D-55

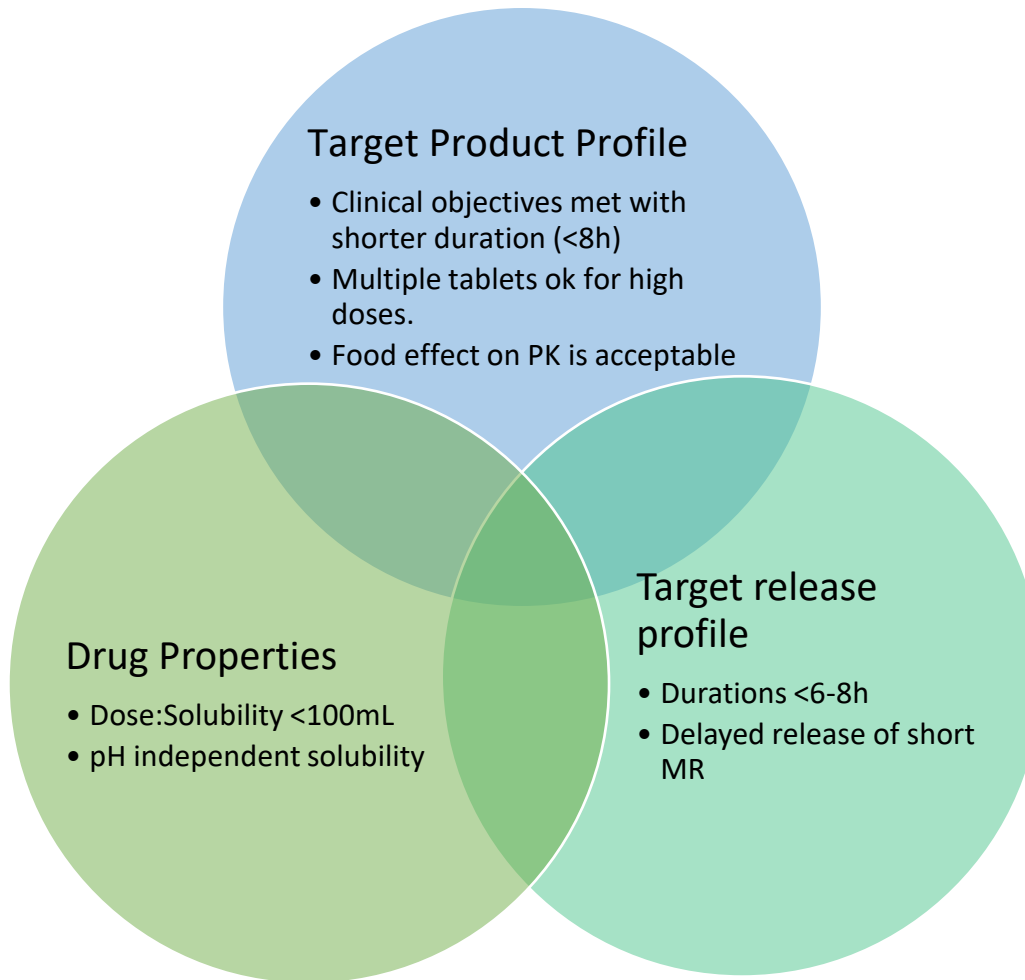


GRALISE® (gabapentin) Pharmacokinetic Mechanism of Action - YouTube

Selection of a CR Technology

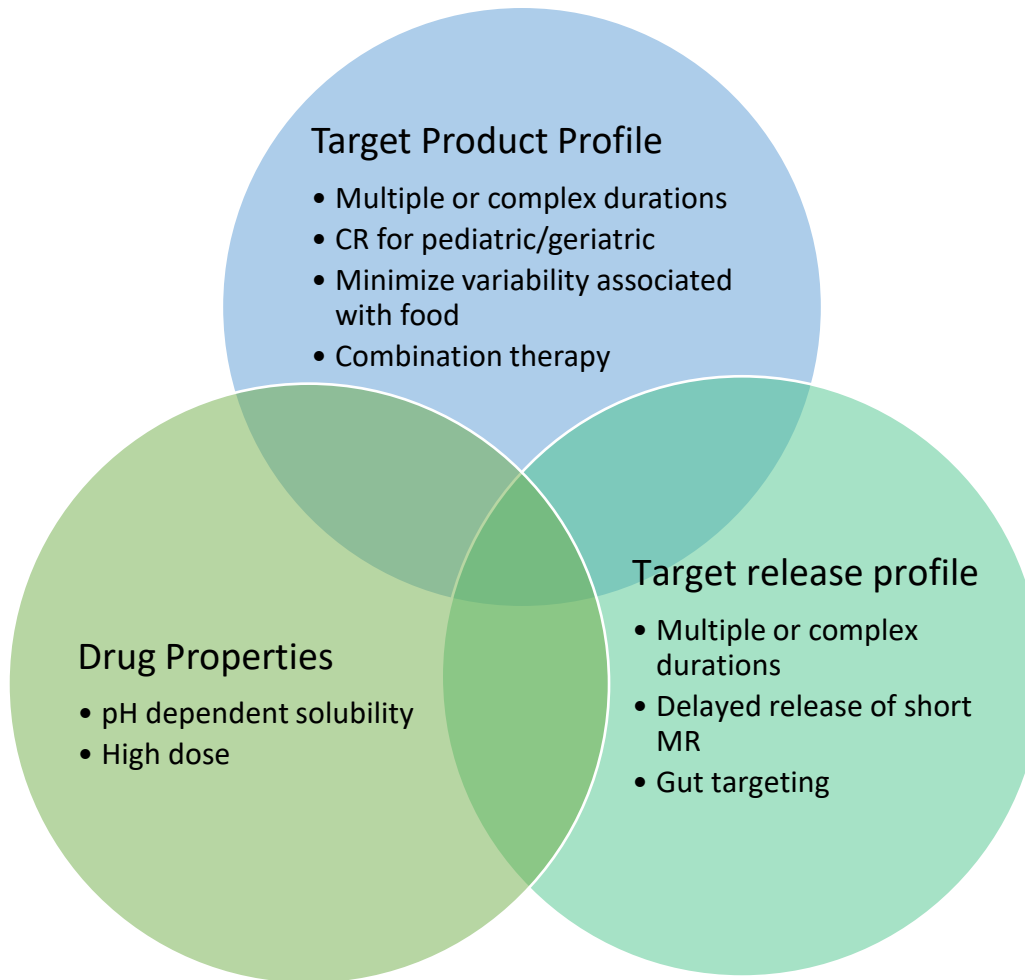


When to use a matrix tablet



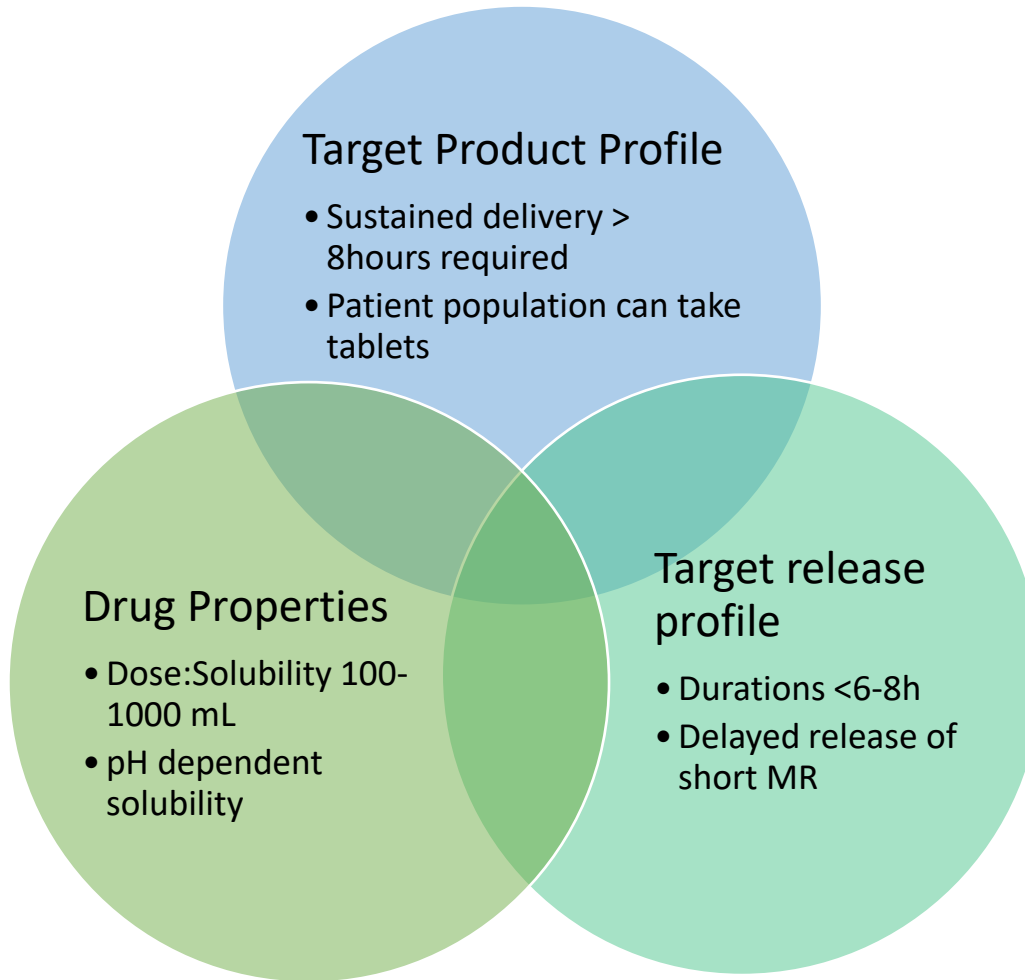
- Matrix tablets are a good starting point:
 - Simple to manufacture
 - Most common marketed CR/MR technology
- Why you might not want to use a matrix tablet:
 - Low drug solubility
 - pH dependent solubility over physiologic range
 - Pediatric/geriatric patients
 - High dose (tablet burden)
 - Combination product

When to use multiparticulates



- Multiparticulates are flexible and versatile:
 - Wide range of profiles
 - Suitable for low and high dose
 - Amenable to different presentations
 - Commercial precedence
- Why you might not want to use multiparticulates:
 - More complex to manufacture than a simple matrix
 - Slower throughput, not continuous (yet)

When to pursue osmotic delivery



- The complexity of an osmotic tablet is worth it when:
 - Narrow therapeutic window
 - Long durations are required to achieve QD dosing
 - Need to minimize iterations of CR design and prototype testing
- When not to use an osmotic tablet:
 - When a simpler technology can achieve the clinical objectives and meet TPP
 - For some geriatric patients and those under 12 years
 - High doses that require multiple tablets

CR Formulation design and optimization tips

- Identify stability/compatibility issues as early as possible
- Start analytical method development early
- Extraction/potency methods can be challenging
- Use sink conditions for formulation optimization
- Low potency is very common due to:
 - Challenges with extraction from blends, granules and tablets
 - Potential for residual drug in tablets
 - Loss of drug during processing

Development and clinical strategy considerations

- Development of CR dosage forms is iterative
- Initial PK studies to establish in vitro and in vivo relationships should use multiple release durations/formulations that bracket design space
- Plan for multiple PK studies to finalize the formulation
- Use of an IR (or IV) as a reference for multiple MR durations in PK studies is recommended
- For drugs with moderate-to-high PK variability, consider the number of subjects/patients for pivotal BA/BE studies

Collaborators

- Leah Appel
- Jeremy Bartlett
- Al Berchielli
- Alan Carmody
- Scott Herbig
- John Larmann
- Michael Roy
- Kazuko Sagawa
- Ravi Shanker
- Avi Thombre
- Ken Waterman